IN THE SPECIFICATION

Please replace the paragraph at page 13, lines 8-17, with the following rewritten paragraph:

First, the layout of an ultrasonic diagnostic equipment 10 according to this embodiment will be described with reference to FIG. 2A. As shown in FIG. 2A, the ultrasonic diagnostic equipment includes an ultrasonic probe 11, a pulser/amplifier unit 13, a waveform control unit 14, an AID converter 15, a detection unit 16, a signal processing unit 17, a filter processing unit 18, a filter processing unit 18, a B-mode processing unit 19, a Doppler processing unit 21, a DSC 23, a display unit 25, and an input unit 27.

Please replace the paragraph at page 18, line 20, to page 19, line 5, with the following rewritten paragraph:

The input unit 27 is connected to the body of the equipment 10, and it is furnished with a control (a mouse or track ball, a mode changeover switch, a keyboard, etc.) for the setting of a region of interest (ROI), etc. in order to accept various instructions, commands and information from an operator into the equipment body 22. Besides, the transmission conditions of the transmission ultrasonic wave can also be manually in the vicinity of a frequency 2f. The reflected wave is equivalent to a wave in which the second harmonic wave of the first fundamental wave as has the center frequency of 2f is broadened onto a higher frequency side so as to enlarge its peak.

Please replace the paragraph at page 23, lines 6-23, with the following rewritten paragraph:

Further, FIG. 7 is a diagram showing the spectrum of a transmission ultrasonic wave which has, for example, two frequency peaks f and 3f. Herein, a fundamental wave which has

its peak at 3f is such that the fundamental wave having its peak at fl in FIG. 3, and the fundamental wave having its peak at f2 in FIG. 5 are added up. In a case where ultrasonic waves having the spectrum have been transmitted to a patient, a reflected wave shown in FIG. 8C, in which the second harmonic wave of the first fundamental wave as shown in FIG. 8A and a difference frequency component (center frequency) shown in FIG. 8B are added up, is measured in the vicinity of a frequency 2f. The reflected wave is equivalent to a wave in which the second harmonic wave of the first fundamental wave [[as]] has the center frequency of 2f [[is]] broadened onto a lower frequency side and a higher frequency side so as to enlarge its peak.

Please replace the paragraph at page 28, line 24 to page 29, line 23, with the following rewritten paragraph:

Concretely, setting as stated below is automatically performed at the step S1. In a case where the difference frequency component is to appear in the vicinity and on the lower frequency side of the frequency of the second harmonic wave of the first fundamental wave (refer to FIG. 3 and FIG. 4), the frequency of the second fundamental wave is set at, for example, 2.8f where f ~~is let denote~~ denotes the frequency of the first fundamental wave. On the other hand, in a case where the difference frequency component is to appear in the vicinity and on the higher frequency side of the frequency of the second harmonic wave of the first fundamental wave (refer to FIG. 5 and FIG. 6), the frequency of the second fundamental wave is set at, for example, 3.2f where f ~~is let denote~~ denotes the frequency of the first fundamental wave. Besides, in a case where the difference frequency component is to appear in the vicinity and on the lower and higher frequency sides of the frequency of the second harmonic wave of the first fundamental wave (refer to FIG. 7 and FIG. 8), the frequency of the second fundamental wave is set at, for example, 3f where f ~~is let denote~~

denotes the frequency of the first fundamental wave. Further, the polarities and amplitudes of the first and second fundamental waves are controlled so as to enhance the second harmonic wave and the difference frequency component each other.

Please replace the paragraph at page 35, lines 9-15, with the following rewritten paragraph:

~~Thenceforth~~Then, substantially the same processing as in the first embodiment is performed, whereby a reflected wave component with a second harmonic component cancelled by a difference frequency component can be extracted at a high accuracy. The extracted contrast medium echo is imaged, whereby useful bio-information can be obtained quickly and easily.